Caffeine Occupancy of Human Cerebral A₁ Adenosine Receptors: In Vivo Quantification with ¹⁸F-CPFPX and PET

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Caffeine is the most commonly consumed psychoactive substance worldwide and an active ingredient in innumerable beverages and foods. Its neurobiologic effects comprise mainly stimulatory actions on alertness, attention (1), cognitive performance (2,3), and cerebral perfusion (4). It is known to reduce sleepiness, to prolong sleep latency, and to enhance wake periods after sleep onset (5,6).

The consumption of approximately 3 cups of coffee corresponds to an oral uptake of 5–8 mg of caffeine per kilogram of bodyweight (7), leading to plasma peak levels of 8–10 mg/L (8,9). The plasma–to–cerebrospinal fluid (CSF) ratio was reported to be 1 for caffeine (10) at equilibrium conditions. CSF concentrations of caffeine will therefore amount to approximately 50 μM (molar weight of caffeine, 194.19 g/mol) after intake of the aforementioned dose of caffeine, which is frequently consumed on a daily basis.

The biologic actions of caffeine are generally assigned to its antagonizing effects at cerebral adenosine receptors. There are 4 different subtypes of adenosine receptors, of which the A₁ adenosine receptor (A₁AR) has the most abundant distribution and highest concentration in the human brain.

Genetic constitutinal knockout animals for the different adenosine receptors suggest that the psychostimulant and arousal effects are mainly mediated by the A₂A adenosine receptor (11–13). However, these data cannot readily be extrapolated to the human condition because there are substantial interspecies differences with regard to the cerebral distribution and concentration of adenosine receptor subtypes. In the human brain, the A₁AR is the most abundant adenosine receptor. It is highly concentrated in human neocortical areas and shows an area- and layer-specific distribution pattern (14) that is strikingly different from its distribution in rodents (15).

The compound 8-cyclopentyl-3-(3-fluoropropyl)-1-propylyxanthine (CPFPX) (14,16) shows a high affinity for the A₁AR (dissociation constant, 1.26 nM in cloned human receptors) and a high selectivity (A₂A adenosine receptor affinity, 940 nM). It has been applied in autoradiographic in...
vitro binding experiments in its tritiated form (\(^{3}\text{H}\)-CPFPX) and in PET experiments as a radiofluorinated compound (\(^{18}\text{F}\)-CPFPX) to determine A\(_{1}\)AR densities in human, non-human primate, and rodent brain tissue. Another PET ligand that has been successfully implemented and has been extensively characterized in humans is the xanthine derivate \(^{11}\text{C}\)-MPDX (17). Because \(^{18}\text{F}\) has a longer half-life than \(^{11}\text{C}\), \(^{18}\text{F}\)-CPFPX is especially suited for bolus–plus–constant-infusion studies with long scan durations.

Various pharmacokinetic modeling approaches have been validated (14,18), and the feasibility of in vivo displacement of \(^{18}\text{F}\)-CPFPX has been shown by an occupancy study with unlabeled CPFPX (19). The proposed models for quantification have a high test–retest reliability and stability (20).

In a recent in vitro study, we measured the concentration of caffeine that displaces 50% of the binding (inhibitory concentration of 50\%, or IC\(_{50}\)) of \(^{3}\text{H}\)-CPFPX to A\(_{1}\)ARs in human postmortem brain tissue (21). The respective IC\(_{50}\) values were in the range of 113–170 \(\mu\text{M}\), implying that the aforementioned commonly consumed doses of caffeine led to an A\(_{1}\)AR occupancy that was accessible in vivo using \(^{18}\text{F}\)-CPFPX and PET. A preliminary PET study with rats served as a proof of principle (22).

The objective of the present study was, therefore, to quantify the in vivo occupancy of A\(_{1}\)AR by caffeine in the human brain with a bolus–plus–constant-infusion paradigm using \(^{18}\text{F}\)-CPFPX and PET.

**MATERIALS AND METHODS**

**Subjects**

All procedures were approved by the Ethics Committee of the Medical Faculty of the University of Duesseldorf, Germany, and the German Federal Office for Radiation Protection. Male volunteers \((n = 15);\text{ mean age, 27.4 ± 3.5 y; age range, 20–34 y}\) participated in this study after having given written informed consent. One subject was scanned twice; thus, a total of 16 displacement studies were analyzed. Volunteers were screened for a history of neurologic and psychiatric diseases, head injury, and alcohol or substance abuse. With the exception of one subject on thyroxin and a second one on antihistaminic medication (fexofenadine), all subjects were without any acute or chronic medication. Caffeine intake was not allowed for at least 36 h before the subjects underwent PET. The chronic daily caffeine consumption was assessed as a multiple of cups (0.15 L) of coffee per day (1 L of caffeine-containing soft drinks was estimated to be equal to \(~1.5\text{ cups of coffee (23).}\)

**MRI Acquisition**

To exclude structural brain abnormalities and to define regions of interest, individual high-resolution MRI datasets were acquired (Magnetom Vision, 1.5 T; Siemens) using a 3-dimensional T1-weighted magnetization-prepared rapid-acquisition gradient-echo sequence (voxel size, 1 \(\times\) 1 \(\times\) 1 mm).

**PET Acquisition**

PET measurements were performed in 3-dimensional mode on an ECAT EXACT HR+ scanner (Siemens-CTI) equipped with a circular lead shield to reduce scatter radiation from outside the field of view (NeuroInsert; Siemens-CTI). Scanning took place with the subjects supine in quiet ambience. The volunteers’ heads were immobilized in the canthomeatal orientation by a vacuum cushion or by customized head shells of polyurethane foam. A 10-min \(^{6}\text{Ge}\)/\(^{80}\text{Ga}\) transmission scan was acquired to correct for attenuation. Head positions were permanently monitored and, if necessary, manually corrected under guidance of a video system and reference skin marks.

A venous catheter in a forearm vein served for tracer application. Arterialized venous blood samples were drawn from a forearm vein contralateral to the injection side. The arm was warmed by heating pads to achieve sufficient arterialization (oxygen saturation > 80%).

Radiosynthesis and formulation of \(^{18}\text{F}\)-CPFPX were performed as previously described (16). The mean specific radioactivity was 75.6 ± 70 GBq/\(\mu\text{mol}\) at the start times of the scans.

\(^{18}\text{F}\)-CPFPX PET was performed according to a bolus infusion schedule as previously described (18). Three slightly different ratios of bolus versus infusion (\(K_{bol}\) time required for injecting the dose of the bolus at a selected infusion rate) were used: 45 min \((n = 6), 48\text{ min (}n = 7),\text{ and 61 min (}n = 3)\). The radioligand was diluted with sterile saline solution (0.9\%) and filled into a 50-\(\mu\text{L}\) syringe. A standard syringe pump was used for tracer application. Dynamic PET acquisition (140 min) in list mode began with the application of the \(^{18}\text{F}\)-CPFPX bolus.

Blood samples were collected at 15-s intervals for the first 2 min; then at 3, 4, 5, 6, 8, and 10 min; and finally at 10-min intervals until 60 min and at 15-min intervals until 140 min. An additional blood sample was taken before \(^{18}\text{F}\)-CPFPX administration, serving for the assessment of the caffeine plasma level.

List-mode data were framed into a dynamic sequence of 9 \(\times\) 30, 3 \(\times\) 60, 3 \(\times\) 150, and 25 \(\times\) 300 s. Slices \((n = 63);\text{ thickness, 2.425 mm; pixel size, 2 \(\times\) 2 mm}\) were reconstructed per time frame by filtered backprojection (Shepp filter, cutoff, 2.5 mm) after Fourier rebinning into 2-dimensional sinograms. Datasets were fully corrected for random coincidences, scatter radiation, and attenuation. The resolution of the reconstructed images varied between 4.1 mm (in full width at half maximum) in the center and 7.8 mm at 20 cm from the center. The sensitivity of the scanner for true events was 5.7 cps/Bq/mL (24).

**Metabolite Analysis**

The activity concentration of the whole blood and plasma (after centrifugation of whole blood for 3 min at 1,000g) was quantified. The fraction of intact radioligand of total plasma activity was determined as previously described (25).

**Caffeine Administration**

Caffeine (Bedford Laboratories) was dissolved in 50 mL of saline (vehicle) and applied with a standard syringe pump as short intravenous infusions between 90 and 100 min. Caffeine concentrations were determined before the start of scanning and additionally in all blood samples from the time of caffeine administration onward. Plasma levels were assessed by high-performance liquid chromatography (in triplicate). Caffeine doses were initially increased in 1 mg/kg steps from 1 mg/kg to approximately 4 mg/kg. However, because the subjects in the upper dose range complained about mild to moderate dizziness and nausea, we did not pursue a further dose escalation. Instead, we attempted to cover the aforementioned dose range in approximately equally spaced dose steps (minor deviations from perfectly equal spacing are caused by the use of a caffeine ampulla of a predefined dosage).
Interactive 3-dimensional image registration software (MPI-Tool, version 3.35; ATV) was used to align individual MRI datasets to the anterior commissure–posterior commissure line. To correct for possible head movements during the acquisition, all frames were realigned to an integrated PET image of the first 10 min using a mutual-information algorithm as implemented in MPI-Tool. The integrated PET frame was then coregistered to the individual MR image, and the resulting parameters were used to coregister the dynamic PET dataset accordingly. Because of the use of customized head shells and rigorous monitoring of patients for possible movements, we encountered only minor movements, which did not exceed the spatial resolution of the scanner. Thus, we made no attempt to realign the individual transmission scans to the emission images.

Volumes of interest were defined by freehand drawing of polygonal regions of interest onto individual MR images using the software package PMOD (version 2.5; PMOD Group). Maximum reproducibility was achieved using identical regions of interest for both conditions. All analyses were performed by a single well-trained investigator using high-resolution MRI data. Thus, interrater variability was avoided. These volumes were used to generate time–activity curves. Time–activity curves were calculated for the following side-averaged cerebral volumes of interest: frontal cortex, orbitofrontal cortex, cingulate gyrus, insula, parietal cortex, occipital cortex, pre- and postcentral gyrus, temporal cortex, mesiotemporal cortex, thalamus, striatum, pons, and cerebellar cortex. Time–activity curves were corrected for the contribution of intracerebral blood volume to the regional activity assuming a fractional blood volume of 5%.

Distribution volumes were calculated using an equilibrium analysis. In the notation of a 2-tissue-compartment model, cerebral 18F-CPFPX concentration can be assumed to be distributed in the intracerebral free and nonspecifically bound (nondisplaceable) (\(C_{ND}\)) compartment and in the specifically bound (placeable) (\(C_S\)) compartment, as well as in a plasma compartment (\(C_P\)). At equilibrium conditions, ligand concentrations in the arterial and venous plasma can be assumed to be equal. The concentration of 18F-CPFPX in venous plasma can therefore be used as a measure of \(C_P\) as has been shown previously (18). The blood volume–corrected tissue time–activity curves summarize \(C_{ND}\) and \(C_S\). Under equilibrium conditions, the total distribution volume (\(V_T\)) is defined as the sum of the nondisplaceable distribution volume (\(V_{ND}\)) and specific distribution volume (\(V_S\)), each composed of \(C_{ND}\) and \(C_S\) related to \(C_P\) (\(V_T = V_{ND} + V_S\) [Eq. 1]).

Parametric images representing \(V_T\) were generated by dividing each frame voxelwise by its corresponding plasma concentration of 18F-CPFPX. Frames were then time-averaged for the baseline and displacement conditions.

**Occupancy Estimation and Estimation of Caffeine IC50**

To estimate the occupancy of A1AR by caffeine, \(V_T\) at baseline (70–90 min) was compared with \(V_T\) after caffeine administration (120–140 min). The fraction of occupancy was determined by the Lassen plot (26,27). This approach is based on the assumption that all regions have identical \(V_{ND}\) estimates. If the reduction in \(V_T\) by the pharmacologic intervention is plotted versus \(V_T\) at baseline, the slope of the resulting regression line corresponds to the occupancy and the \(y\)-axis intercept to \(V_{ND}\). True equilibrium conditions have to be fulfilled during baseline and displacement estimations of \(V_T\) to gain valid estimates of \(V_T\) and, consequently, of fractional occupancy and \(V_{ND}\).

On the basis of the occupancy estimates from the Lassen plot, the IC50 can be determined by fitting the occupancy data versus the corresponding plasma caffeine concentration using the following formula:

\[
\text{Occupancy} = \frac{\text{(caffeine dose)}}{(\text{IC50} + \text{caffeine dose})}. \quad \text{Eq. 1}
\]

**RESULTS**

**18F-CPFPX Bolus Infusion**

Mean injected radioactivity was 346 ± 49 MBq (range, 220–370 MBq). The quantity of injected CPFPX was 17.5 ± 18.7 nmol (range, 1.6–66 nmol). The mean rate of change of the concentration of parent compound between 50 and 90 min was 6.4% ± 8.3%/h. Figure 1 depicts the time course of 18F-CPFPX in plasma and the respective concentration in cerebral tissue in a representative subject. The steady state of 18F-CPFPX in plasma and tissue was achieved 40–50 min after the start of injection. On infusion, caffeine displaced 18F-CPFPX rapidly in all brain regions. It also led to an increase of the plasma concentration of 18F-CPFPX (Fig. 1) by competitive inhibition of CYP1A2 (as previously described in the studies by Meyer et al. (18) and Matusch et al. (28)). The tissue-to-plasma ratio (reflecting \(V_T\) during equilibrium) attained steady-state conditions after 60–70 min. Average regional \(V_T\) estimates, based on the tissue-to-plasma ratio between 70 and 90 min, can be found in Table 1. The \(V_T\) values found in the present study are in agreement with previously reported values (18).

**Caffeine Plasma Levels**

There is a highly significant, linear relationship (\(r = 0.94, P < 10^{-8}\)) between intravenously applied caffeine doses (per body weight) and attained caffeine plasma concentrations (Fig. 2, left). The time course of plasma caffeine concentrations is displayed on the right graph in Figure 2.

![Image](http://example.com/image1.png)

**FIGURE 1.** Representative regional time–activity curves and corresponding concentration of unmetabolized 18F-CPFPX in plasma in subject who received highest dose of caffeine and showed highest displacement (caffeine challenge at 90–100 min with a dose of 4.3 mg/kg of body weight).
After an initial distribution phase, stable caffeine levels were observed from 120 min onward. This observation is in line with the terminal half-life of caffeine of approximately 5–6 h. Caffeine doses in the range of 0–9 mg/L were achieved at a time point of 120 min, which was used for further estimations of IC50 values.

Impact of Caffeine on 18F-CPFPX VT and Estimation of Caffeine IC50

Caffeine displaced 18F-CPFPX in a dose-dependent manner. Parametric images of VT of 1 subject before and after caffeine administration are shown in Figure 3. Representative time courses of the apparent VT after various doses of caffeine are plotted in Figure 4. The vehicle did not significantly affect VT. Caffeine led also to a dose-dependent reduction of VT in the cerebellum, the region with the lowest binding in the human brain. Maximum VT displacement in the cerebellum was 33% at the highest caffeine dose.

Lassen plots and fits of all subjects are displayed in Figure 5. The maximum occupancy achieved in this study was 44% (4.27 mg/kg). Cerebral A1AR occupancy was clearly dependent on the plasma caffeine level (Fig. 6). According to Equation 1, the IC50 of caffeine amounted to 12.5 mg/L (SE of fit, 1.5 mg/L). VND based on the Lassen plot (x-axis intercept) was 0.11 ± 0.10, which corresponds to one quarter of the average cerebellum VT.

DISCUSSION

Caffeine is the most commonly and broadly used neurostimulant. Therefore, it is a longstanding desire in neuroscience and addiction research to investigate the effects of caffeine directly in the human brain. We used the PET tracer 18F-CPFPX to visualize and quantify the occupancy of the A1AR, the most abundant caffeine target in the human brain. The present study demonstrates that 18F-CPFPX is highly displaceable by caffeine and allows the determination of the occupancy of A1ARs by caffeine in vivo and in a quantitative manner.

On the basis of the present PET study, the IC50 of caffeine amounts to approximately 13 mg/L, corresponding to about 67 μM caffeine in plasma. This value can be extrapolated to an oral caffeine intake of 450 mg in a 70-kg subject, which corresponds to approximately 4–5 cups of coffee. It is therefore likely that usually consumed amounts of coffee and caffeinated beverages (29) result in brain concentrations of caffeine that block substantial portions of cerebral A1ARs. Because A1ARs are quantitatively the most important neocortical binding sites of caffeine in the human brain, it is likely that the cognition-enhancing effects of caffeine are exerted by this adenosine receptor subtype. With regard to future A1AR PET studies, it is important to keep in mind that acute caffeine consumption will severely bias quantitative A1AR PET measurement. Thus, a sufficiently long caffeine abstinence is mandatory before scanning.

This is the first, to our knowledge, in vivo study on cerebral A1AR occupation by caffeine in humans. Therefore, it is interesting to compare our results with previous in vitro investigations. We recently determined the IC50 of caffeine in human postmortem frontal cortex homogenates. Using 3H-CPFPX, the tritiated analog of 18F-CPFPX, we

<table>
<thead>
<tr>
<th>Region</th>
<th>VT</th>
</tr>
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<tbody>
<tr>
<td>Cerebellum</td>
<td>0.45 ± 0.08</td>
</tr>
<tr>
<td>Pons</td>
<td>0.46 ± 0.10</td>
</tr>
<tr>
<td>Thalamus</td>
<td>0.82 ± 0.16</td>
</tr>
<tr>
<td>Precentral gyrus</td>
<td>0.68 ± 0.13</td>
</tr>
<tr>
<td>Postcentral gyrus</td>
<td>0.72 ± 0.13</td>
</tr>
<tr>
<td>Cingulate gyrus</td>
<td>0.72 ± 0.15</td>
</tr>
<tr>
<td>Orbitofrontal gyrus</td>
<td>0.75 ± 0.14</td>
</tr>
<tr>
<td>Parietal cortex</td>
<td>0.79 ± 0.17</td>
</tr>
<tr>
<td>Occipital cortex</td>
<td>0.92 ± 0.02</td>
</tr>
<tr>
<td>Insula</td>
<td>0.70 ± 0.15</td>
</tr>
<tr>
<td>Mesiotemporal cortex</td>
<td>0.65 ± 0.13</td>
</tr>
<tr>
<td>Striatum</td>
<td>0.83 ± 0.15</td>
</tr>
<tr>
<td>Frontal cortex</td>
<td>0.77 ± 0.16</td>
</tr>
<tr>
<td>Temporal cortex</td>
<td>0.80 ± 0.14</td>
</tr>
<tr>
<td>Caudate nucleus</td>
<td>0.74 ± 0.16</td>
</tr>
<tr>
<td>Putamen</td>
<td>0.84 ± 0.17</td>
</tr>
</tbody>
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Data are mean ± SD.
determined the in vitro IC$_{50}$ to be in the range of 113–170 µM. To compare these values with the in vivo data, assumptions about the biodistribution of caffeine have to be made because no human data on intercellular caffeine accumulation are available. The ratio of plasma caffeine to CSF caffeine is close to 1 in rats (10). Assuming the cellular conditions in humans and rats are comparable in this respect, the IC$_{50}$ for plasma will then lead to a CSF concentration of 67 µM, which is about half the in vitro value. This discrepancy might be caused by species differences in the plasma-to-CSF ratio, the in vivo versus the in vitro settings of the experiments, or postmortem changes. Besides these technical reasons, the presence of caffeine metabolites, which are probably also binding to the A$_1$AR, might explain the difference between in vivo and in vitro conditions as well. For instance, theophylline binds to A$_1$ARs with a $K_i$ (binding affinity of the inhibitor) of 8.5 µM (30), and theobromine, another metabolite, has a $K_i$ comparable to that of caffeine (97–197 µM) (31). Finally, incomplete kinetic equilibration after caffeine administration may also contribute to a possible underestimation of the IC$_{50}$: although stable concentrations of $^{18}$F-CPFPX in plasma and the cerebral compartment were attained at baseline (70–90 min), plasma concentrations of $^{18}$F-CPFPX rose after caffeine administration. This increase of plasma concentration is most likely caused by competitive inhibition of caffeine and CPFPX at their common hepatic enzyme CYP1A2 (18,28). The changed equilibrium of

FIGURE 3. Representative parametric images of total distribution volume of 1 subject at baseline (average from 60 to 85 min, middle) and after 4.1 mg/kg dose of caffeine (average from 115 to 140 min, bottom). Corresponding anatomic MR images, with overlay of regions of interest, were used for analysis (top).

FIGURE 4. Dose-dependent displacement of $^{18}$F-CPFPX by caffeine in frontal cortex. $V_T$ is plotted vs. time for 4 subjects who received different doses of caffeine or vehicle at 90–100 min. For visualization purposes, $V_T$ was normalized to mean of 75–90 min.
$^{18}$F-CPFPX in plasma and tissue may accordingly not have been fully attained between 120 and 140 min (Fig. 1, precentral gyrus). Because the cerebral kinetics of $^{18}$F-CPFPX may be delayed relative to plasma kinetics, $V_T$ could be overestimated during displacement, resulting in an underestimation of IC$\text{_{50}}$. However, available data up to 140 min suggest that the underestimation is less than 5%.

The present estimate of $V_{ND}$ from the Lassen plots is relatively low ($V_{ND}$, 0.11 ± 0.10), corresponding to about one quarter of the cerebellar $V_T$. In an earlier $^{18}$F-CPFPX displacement study using unlabeled CPFPX, $V_{ND}$ was about two thirds of the $V_T$ of the cerebellum (19). Again, incomplete equilibration might be accountable for this difference. In a previous study, we have carefully evaluated changes of specific binding in the reference region with regard to their effects on noninvasive outcome parameters such as the binding potential (20). We also investigated the constraints for using the cerebellum as a reference region, which allows omitting blood sampling and reduces the additional noise introduced by blood analyses.

In the field of neuroimaging (especially the blood oxygen level–dependent [BOLD] contrast imaging–functional MRI), caffeine is known to lower the resting state or baseline BOLD signal (32). It is likely that the observed caffeine effects on the BOLD contrast are a combination of the increased neuronal activation (33) through a disinhibitory mechanism at the A$\text{1}_AR$ and a reduction of the cerebral blood flow (34) by inhibition of vascular A$\text{2}_A$ adenosine receptors. The present method of A$\text{1}_AR$ occupancy measurements with $^{18}$F-CPFPX, by providing individual data of A$\text{1}_AR$ densities and acute caffeine effects in a regional and quantitative manner, could help to solve current inconsistencies in findings related to caffeine and functional MRI (32).

An important finding of the present study is that in most regular consumers of caffeine, about half of the cerebral A$\text{1}_AR$s may be occupied by caffeine. It is likely that this phasic blockade of a substantial amount of cerebral A$\text{1}_AR$s will result in adaptive changes and lead to chronic alterations of receptor expression and availability. There is substantial epidemiologic evidence that caffeine is protective against neurodegenerative diseases such as Parkinson or Alzheimer disease. Several investigations (e.g., the Cardiovascular Risk Factors, Aging and Dementia study) show that moderate coffee consumption of 3–5 cups per day at mid life is linked to a smaller risk of dementia in late life (35). The present study provides evidence that typical caffeine doses result in a high phasic receptor occupancy, which will most likely induce chronic cerebral, especially neocortical, A$\text{1}_AR$ changes. These findings support the view that the A$\text{1}_AR$ deserves broader attention in the context of neurodegenerative disorders. Further studies will be needed to investigate the precise interplay of age, adenosine receptors, and neurodegenerative pathophysiology.

**CONCLUSION**

This study demonstrates that caffeine occupancy studies of the cerebral A$\text{1}_AR$ can be performed with $^{18}$F-CPFPX bolus–plus–constant-infusion PET protocols. Our data provide evidence that repeated intake of caffeinated...
beverages results in a 50% occupancy of the cerebral A1AR during longer periods of the day. 18F-CPFPX PET represents a valuable technique for studying the neurostimulant and chronic neuroplastic effects of caffeine in humans.

DISCLOSURE STATEMENT

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